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Positron emission tomography (PET) and singlephoton-emission computed tomography (SPECT) are important nuclear medicine modalities that have been ⁴⁰ widely used for clinical diagnosis. PET detects the coincidence of annihilation gamma-rays from a positronemitting nuclide. SPECT uses a collimator to restrict the incident direction of gamma-rays. Therefore, nuclides for ⁴⁰ PET imaging are limited to positron-emitting nuclides and there is a theoretical spatial resolution limit derived from the positron range. The sensitivity of SPECT is relatively low because of its use of a collimator, and it is difficult to image multiple nuclides simultaneously. To realize highly sensitive multi-nuclide imaging, we proposed a double-photon -emission coincidence imaging method.¹

For SPECT imaging, single-photon-emitting nuclides are preferable. Among them, there are nuclides that emit two photons in cascade decay. For example, ¹¹¹In, which is widely used in SPECT imaging, emits two gamma-rays at 171 keV and 245 keV. Using two gammarays, the position of nuclides can be determined with higher sensitivity. One of the methods using two gammarays is double-photon-emission computed tomography (DPECT).^{1,2)} This method can drastically increase the signal-to-noise (SN) ratio of Compton $\text{imaging}^{3)}$ by coincidence detection for cascade gamma-rays with multiple Compton cameras, which is based on Compton scattering kinetics. Conventional Compton imaging can obtain only the angle information of incident gamma-rays, and drawing many Compton cones results in a low SN ratio. However, DPECT can limit the nuclide position from a Compton cone to an overlap of two Compton cones. We previously demonstrated DPECT using $^{134}\mathrm{Cs}$ and $^{60}\mathrm{Co}$ for application to fuel debris imaging²) with GAGG-SiPM Compton cameras.⁴⁾ In the present research, we developed small GAGG-SiPM Compton cameras for application to nuclear medicine and demonstrated doublephoton-emission coincidence methods using ⁴³K, which is one of the promising double-photon-emitting nuclides because of its short decay time and suitable gamma-ray



Fig. 1. Experimental setup of DPECT for 43 K.

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Single-Compton imaging (a) 373keV (b) 617keV (C) Time difference of DPECT (b) 617keV (c) Time difference of DPECT (c) Time



energies.

 43 K was produced in the 43 Ca $(d, 2p)^{43}$ K reaction at the RIKEN AVF cyclotron. After chemical separation, 2 (6) MBq of 43 K in 6 (18) μ L H₂O was placed in a vial as a gamma-ray source. Figure 1 shows the experimental setup of DPECT for ⁴³K. ⁴³K mainly emits cascade gamma-rays at 617 keV and 373 keV. A Compton camera consists of a scatter layer and an absorber layer. Each layer consists of an 8×8 GAGG array coupled to an 8×8 SiPM array. The thicknesses of the GAGG arrays is 4 mm and 9 mm for scatterers and absorbers, respectively. The pixel size of the GAGG arrays is $2.5 \text{ mm} \times 2.5 \text{ mm}$, and each crystal is separated by BaSO₄ reflectors. The signal from SiPM is processed by the dynamic time over threshold (dToT) method⁵⁾ to extract the energy. The distance from the 43 K source to a scatterer was 30 mm, and two Compton cameras were placed in opposite directions.

Figures 2(a) and 2(b) show images reconstructed through back projection. Figure 2(a) shows a singlephoton Compton image at 373 keV and (b) shows an image at 617 keV. We succeeded in obtaining images of single-photon Compton imaging with our small Compton cameras. Figure 2(c) shows a histogram of time difference of double Compton coincidence events at 373 keV and 617 keV. However, the number of coincidence events that can be used for DPECT with Compton scattering energy windows was only 12. After this experiment, we increased the number of Compton cameras to detect double Compton coincident events efficiently and repeated the experiment with eight modules. The result is under analysis.

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